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A multi-joint lower-limb tracking-trajectory test for the assessment of motor coordination

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Abstract c

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This study aimed to determine whether a lower-limb trajectory-tracking task performed on a leg press machine, that is commonly adopted in 10 both rehabilitation and resistance training settings, could yield reliable assessment of motor coordination in able-bodied individuals. Twenty-11 two female subjects allocated to two experimental groups were tested and retested after 48-72 h. Group A was fully familiarized with the 12 experimental procedures before each test while group B received only verbal instructions. The unilateral coordination test consisted of target 13 tracking during a simulated half squat including eccentric and concentric actions. In both groups, tracking error showed significant test-retest 14 reliability with ICC values of 0.77–0.80 (p < 0.05). Significant group (A < B) and time (day 2 < day 1) main effects were found for tracking 15 error, while there was no significant influence of action mode and dominance. Tracking error significantly decreased in the group A (~15%) 16 but not in the group B on retest. Action mode (eccentric versus concentric), side dominance and familiarization on day 1 had no effect on 17 tracking error. However, movement control significantly improved at day 2, thus confirming the occurrence of short-term motor learning and 18 the sensitivity of the present trajectory-tracking test. For the first time, a simple test for the assessment of motor coordination during multi-joint 19 closed-kinetic chain action of lower limb muscles has been proposed. Its uniqueness is represented by the specificity for rehabilitation and 20 resistance training settings. Further studies with larger sample groups (e.g., male subjects and patients) and including neurophysiological 21 measurements are needed. 22 © 2005 Published by Elsevier Ireland Ltd. 23

Keywords: Coordination; Leg press; Tracking ability; Motor learning 24

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Trajectory-tracking tasks are commonly used in healthy in-26 dividuals and in persons with movement disorders for quan-27 titating movement control (i.e., motor coordination [17] or 28 motor skill [15]) during a single joint movement, such as fin-29 ger or elbow flexion-extension. This technique has proven 30 useful to investigate the effect of age [7,19], gender [7], fa-31 tigue [15], training [2,6], and also central nervous system 32 impairment [14] on tracking accuracy. Carey et al. [7] also 33 demonstrated that in healthy subjects the nonpreferred (non-34 dominant) hand tracked more accurately than the preferred 35 hand. Less information is however available on tracking con-36 trol during the flexion compared to the extension phase of a 37

test [7], i.e., during shortening (concentric) versus lengthening (eccentric) muscle actions.

The majority of the studies investigating tracking perfor-40 mance have focused on movements about a single joint of 41 the upper extremities, whereas, to our knowledge, lower-limb 42 trajectory-tracking task was considered only in one instance 43 [6]. These authors examined the ability of one stroke patient to perform accurately controlled plantar flexion and dorsiflexion (open kinetic chain) movements with a single joint ankle test. Surprisingly, tracking ability during multi-joint closed-kinetic chain actions of the lower limb muscles has never been analysed to date, even if activities of daily living, that require the ability of movement control in addition to 50 force control, are mostly performed in these conditions, par-51 ticularly for the muscles involved in maintaining posture and 52 balance. Consequently, it is reasonable to verify the feasibility 53

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of a specific trajectory-tracking test involving the participa tion of the most important lower limb extensor (agonist) and
 flexor (antagonist) muscles.

The first aim of this study was to determine whether a 57 lower-limb trajectory-tracking task performed on a commer-58 cially available horizontal leg press machine, that is com-59 monly adopted in both rehabilitation and resistance training 60 settings, could yield reliable assessment of motor coordina-61 tion in able-bodied female individuals. To address this prob-62 lem, we used a simple test-retest design and evaluated the 63 basic properties of the trajectory-tracking task. 64

Based on previous research on tracking ability assessment, 65 we also tested the following hypotheses: (i) the non-dominant 66 lower limb would track more accurately than the dominant 67 [7]; (ii) accuracy in the concentric phase of the movement (ex-68 tension) would be higher than during the eccentric (flexion) 69 phase; (iii) very short-term (warm-up before the first session) 70 and short-term (second versus first session) learning effect 71 over a limited number of trials would improve trajectory-72 tracking accuracy [9]. 73

Twenty-two healthy and physically active female subjects
volunteered to participate in this study. They gave written,
informed consent before the experiment and the approval for
the project was obtained from the Local Committee on Human Research (Schulthess Klinik, Zürich, Switzerland). The
study was conducted according to the Declaration of Helsinki
(last modified in 2000).

Participants were instructed to refrain from strenuous 81 physical activity for 24 h prior to testing and to maintain 82 normal exercise levels throughout the period of the exper-83 iment. They were randomly allocated to two experimental 84 groups (n = 11 for both): group A (mean age \pm S.D.: 28 ± 3 85 years; height: 169 ± 5 cm; mass: 58 ± 7 kg) and group B (age: 86 27 ± 3 years; height: 169 ± 5 cm; mass: 62 ± 10 kg). All sub-87 jects were tested and retested (mean interval between day 88 1 and day 2: 48-72 h) for tracking ability assessment on a 89 commercially available horizontal leg press machine (Func-90 tional Squat System, Monitored Rehab Systems, Haarlem, 91 The Netherlands), as detailed below. The movement consid-92 ered is a 'simulated' one-leg half-squat, starting from a supine 93 position, with the hip, knee and ankle joints flexed at $\sim 90^{\circ}$. 94 The load (range 0–100 kg) is raised during the first phase by 95 concomitant hip, knee and ankle extension (i.e., concentric 96 contraction of the main lower limb extensor muscles) until 97 the knee joint is fully extended. This is followed by the flexion 98 phase, where the same (agonist) muscle groups are stretched gq (i.e., eccentric action) while the antagonist flexor muscles are 100 coactivated during the entire half squat movement. Through-101 out this paper, the terms concentric and eccentric will be used 102 instead of flexion and extension, respectively, and will refer 103 to the action of the main hip (gluteus maximus), knee (quadri-104 ceps femoris) and ankle (triceps surae) extensor muscles. The 105 machine is connected to a personal computer and a dedicated 106 software provides real-time and off-line data analysis. Indi-107 viduals from both groups completed a familiarization phase 108 (duration: 5 min) before the coordination test, with group A 109

(but not group B) also completing a standardised warm-up (duration: 15 min) in the two occasions (i.e., days 1 and 2), aimed at improving motor learning. All testing sessions were conducted by the same experimenter (SS) and at the same time of day. Positioning adjustments on the horizontal leg press machine were recorded on laboratory form to aid in reproducing the subject setup for the retest session.

During the familiarization phase, the subjects were correctly positioned in the leg press machine (supine with the hip, knee and ankle joints flexed at $\sim 90^{\circ}$), and verbal instructions were provided on how to perform the coordinative test. The examiner then offered advice and answered any further questions but subjects were not allowed practice trials.

For the group A, warm-up (very short-term motor learn-123 ing) consisted of four series of 10 concentric-eccentric rep-124 etitions at the leg press machine, performed unilaterally (for 125 both lower limbs), with 1 min rest between each series. The 126 range of motion at the knee joint was $\sim 90^{\circ}$ and the load was 127 comprised between $\sim 1/6$ (16.6%) and $\sim 1/3$ (33.3%) of the 128 individual body mass. Then, the load was adjusted to $\sim 1/10$ 129 (10%) of the body mass, i.e., 5 kg, and subjects were allowed 130 one-two 30s practice trial of the coordinative test (see be-131 low), with both the dominant and non-dominant lower limb. 132 The dominant lower limb was determined for each subject by 133 asking which lower limb she would use to kick a ball with as 134 far as possible [13]. 135

The coordination test was completed unilaterally with a 136 load minimizing force control (5 kg, \sim 10% of body mass), 137 and consisted of 60s of target tracking during eccentric-138 concentric contractions of the lower limb muscles. Subjects 139 were provided ongoing visual feedback of their position by 140 means of a cursor (a sort of target) displayed on a video moni-141 tor in front of them. They were instructed to match a criterion 142 trajectory (see Fig. 1) as accurately as possible, minimizing 143 the difference between their performance and the criterion. 144 With the exception of the first and last few seconds, the ma-145 jority of the test was performed with a knee angle comprised 146 between 70 and 10° of flexion. No feedback or advice was 147 given by the examiner both during and at the end of the test. 148 All the subjects performed the task with the dominant and the 149 non-dominant lower limb and the test order was randomised. 150 For each condition, two trials were completed and the aver-151 age value of the two scores was retained for data analysis. 152 Adequate rest periods (>1 min) were allowed between trials. 153

Tracking accuracy was quantified as proposed by the man-154 ufacturers of the Functional Squat System. The software cal-155 culated automatically the absolute average error (in cm), i.e., 156 average of actual trajectory minus criterion trajectory for each 157 data point, and the standard deviation (S.D.) of the average 158 error. Both average and S.D. error were independently quan-159 tified as a function of the action mode (concentric versus 160 eccentric) and of the tested lower limb (dominant versus non-161 dominant). 162

A four-way ANOVA with repeated measures on the last three factors was performed to study the effect of group (A versus B), dominance (dominant versus non-dominant lower

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Fig. 1. A schematic representation of the tracking test used in this study. The concentric and eccentric phase, the criterion trajectory (thick line) and the actual position of the target at the beginning, in the middle and at the end of the test are also represented.

limb), action mode (eccentric versus concentric) and time 166 (day 1 versus day 2, i.e., short-term motor learning) on de-167 pendent variables. When significant effect or interaction oc-168 curred, Tukey post hoc analyses were used to test differences 169 among means. Test-retest reliability between day 1 and day 2 170 values was assessed by calculating a Pearson product corre-171 lation coefficient (r) and an intraclass correlation coefficient 172 (ICC) using the ICC(2, k) model, as described by Shrout 173 and Fleiss [18]. The ICC, which is a measure of correlation 174 that considers variance, describes the agreement between the 175 repeated measures. We used also the standard error of the 176 measurement (SEM) to indicate absolute reliability and cal-177 culated it according to Atkinson and Nevill [1]. For all mea-178 sures of reliability, dominant and non-dominant lower limb 179 values were collapsed. The level of significance was set at 180 p < 0.05 for the ensemble of the procedures. The statistical 181 analyses were undertaken by using Statistica 6.0 (StatSoft 182

Table 1

Test-retest reliability (Pearson product correlation coefficient, r; intraclass
correlation coefficient, ICC; standard error of the measurement, SEM) of
average and S.D. error in the two experimental groups

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Average error	S.D. error	
$r = 0.715^*$ ICC = 0.824^{**} SEM = 0.023 cm	$r = 0.714^*$ ICC = 0.796 ^{**} SEM = 0.053 cm	
r = 0.446 ICC = 0.590 SEM = 0.028 cm	$r = 0.808^{**}$ ICC = 0.771* SEM = 0.064 cm	
	Average error $r = 0.715^*$ ICC = 0.824** SEM = 0.023 cm $r = 0.446$ ICC = 0.590 SEM = 0.028 cm	

* p < 0.05.

** p < 0.01.

Inc., Tulsa, Usa) and SPSS 11.0 (SPSS Inc., Chicago, Usa) for Microsoft Windows.

In group A, both average and S.D. error showed significant 185 test-retest reliability (Pearson's r: p < 0.05; ICC: p < 0.01; 186 Table 1), even if subjects from this group significantly en-187 hanced their accuracy at the coordinative test performed on 188 day 2. On the other hand, test-retest reliability was significant 189 for S.D. error (Pearson's r: p < 0.01; ICC: p < 0.05), but low 190 and insignificant for average error (Table 1) in those subjects 191 who were not accustomed with the test (group B). Compar-192 ison of the SEM values with the calculated means indicated 193 that the SEM values were relatively small for S.D. error but 194 quite high for average error in both groups. 195

No significant main effects or interactions were found for average error (Table 2 and Fig. 2A), even if a tendency was observed for time (day 2 < day 1) and for time by action mode (p = 0.084).

Significant group (A < B) and time (day 2 < day 1) main 200 effects were found for S.D. error (Table 2), while there was 201 no significant influence of action mode and dominance. S.D. 202 error showed a significant group by time interaction (F = 4.37, 203 p = 0.039). Post hoc analyses evidenced that, at day 2, S.D. 204 error significantly decreased in the group A (\sim 15%) but not 205 in the group B (p < 0.001, Fig. 2B). Moreover, S.D. error of 206 group A at day 2 was significantly lower than day 1 (p < 0.001) 207 and also than group B values at day 2 (p = 0.028). 208

Table 2

F-values and p-levels for main effects associated to the 4-way ANOVA on average error and S.D. error

Variable	Main effect	<i>F</i> -value	p-level
Average error	Group	0.38	0.539
	Dominance	0.45	0.505
	Action mode	0.66	0.418
	Time	3.14	0.080
S.D. error	Group	5.28	0.024
	Dominance	0.09	0.760
	Action mode	0.05	0.823
	Time	11.93	0.0009

No significant interactions were found for average error. A significant group \times time interaction was observed for S.D. error (see text and Fig. 2B for details).

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Fig. 2. Average error (A) and S.D. error (B) in the two experimental groups at days 1 and 2. Data (mean and S.D.) are collapsed for action mode and lower limb. (***) Significantly lower than day 1 (p < 0.001); ([†]) significantly lower than group B at day 1 (p < 0.05); (^{†††}) significantly lower than group B at day 2 (p < 0.05).

The trajectory-tracking test proposed in the present study 209 represents a good tool for the evaluation of motor coordi-210 nation during multi-joint closed-kinetic chain action of the 21 lower limb musculature. High test-retest reliability was ob-212 served for S.D. error but not for average error in the group 213 of subjects considered unaccustomed. The obtained results 214 suggest that action mode (eccentric versus concentric), side 215 dominance and warm-up (very short-term motor learning) 216 did not influence the outcome measure, therefore invalidating 217 our preliminary hypotheses. However, S.D. error was signif-218 icantly improved after one testing session, thus confirming 219 the occurrence of short-term motor learning and the sensitiv-220 ity of the present trajectory-tracking test. On the other hand, 221 average error is probably not sensitive enough to detect sig-222 nificant improvement in tracking accuracy. 223

In the current study, intersession reliability was studied by correlating the average and S.D. error obtained at day 1 with respect to day 2 for both experimental groups. However, even though participants from group A were accustomed with the trajectory-tracking test – since their S.D. error significantly decreased from session to session ($\sim 15\%$) – both average 229 and S.D. error showed significant Pearson's r values and ICC 230 values, therefore suggesting that the improvement was quite 231 homogeneous for this subjects group. On the other hand, in 232 group B – that was considered unaccustomed to the experi-233 mental test – reliability for S.D. error was quite high, while 234 it was low and insignificant for average error. Together with 235 SEM values, these findings indicate that S.D. error should be 236 preferred to average error to characterise tracking accuracy 237 in future studies. It is indeed possible that the poor reliability 238 of average error is explained by the very low values (near to 239 zero) associated to this parameter, as a result of the 'average' 240 actual trajectory with respect to the 'average' criterion tra-241 jectory shown in Fig. 1. Therefore, an average error equal to 242 zero should not necessarily be associated to an accurate test, 243 since the concomitant S.D. error should be extremely high. 244

Tracking accuracy is typically quantified as the root-mean-245 square error between the criterion and the performance tra-246 jectory, this error being subsequently normalised to the total 247 range of motion to give an accuracy index [8]. In our study, 248 even though absolute S.D. error was quantified as the dis-249 placement of the leg press load (in cm), it is important to 250 note that, due to the homogeneous composition of the present 251 experimental groups, the same results were obtained when 252 absolute S.D. error was normalised to the individual range of 253 motion (group A: day 1: 2.62% and day 2: 2.16%; group B: 254 day 1: 2.76% and day 2: 2.65%). 255

It was hypothesised that action mode would have influenced the outcome of our trajectory-tracking test, i.e., accu-257 racy in the concentric phase of the movement would have 258 been higher than under eccentric conditions. However, it was 259 not the case. Our hypothesis was based on the fact that eccen-260 tric contractions are distinctly controlled by the central ner-261 vous system [11], with lower discharge rate and recruitment 262 of fewer motor units with respect to concentric actions, which 263 in turn result in greater fluctuations in acceleration [10], and 264 therefore in lower movement accuracy. However, the fact that 265 the absolute load adopted in this study was the same during 266 eccentric and concentric actions (5 kg), while maximal volun-267 tary strength at a given velocity is considerably higher in the 268 former conditions, inevitably affected movement control dur-269 ing the extension phase of trajectory-tracking task. It is then 270 possible that such an advantage during the eccentric phase of 271 the movement was compensated by the neural disadvantage 272 of lengthening contractions. 273

According to previous research on finger control [7,12], 274 we also hypothesised that limb dominance would have af-275 fected the results of the present trajectory-tracking test, i.e., 276 the non-dominant lower limb (the left for the majority of our 277 subjects) would have tracked more accurately than the dom-278 inant. Hypothesis was also based on the fact that tracking 279 skill requires processing of visuoperceptual and visuospatial 280 relationships for which the right hemisphere is more special-281 ized [4]. No difference was however observed between the 282 two sides. It is indeed possible that the differences previously 283 reported between preferred (or dominant) and nonpreferred 284

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side could not be extended to the lower extremities, mainly 285 because of the respective solicitation during daily living ac-286 tivities, i.e., upper limbs are used more asymmetrically than 287 lower limbs. 288

No difference was observed between the two experimen-289 tal groups at day 1, i.e., there were no very short-term motor 290 29 learning effects (warm up) on tracking accuracy. Significant improvements were however observed for S.D. error but not 292 for average error at day 2 in those subjects who were well 293 accustomed with the experimental protocol (group A). These 294 findings confirm that a limited number of trials result in a 295 significant improvement of tracking ability in healthy indi-296 viduals through short-term motor learning [9]. These results 297 also clearly demonstrate the sensitivity of S.D. error but not of 298 average error to detect enhancement of tracking performance 299 with repeated trials. Even though additional experiments are 300 needed to evaluate sensitivity as well as intrasession relia-301 bility in larger groups (including healthy male subjects) and 302 in individuals with movement disorders, the manufacturer 303 should consider revising the variables provided by the soft-304 ware. 305

The unique aspect of our current study is the specificity of 306 the trajectory-tracking test for rehabilitation and resistance 307 training settings, but also for several activities of daily liv-308 ing. In 1988, Carey et al. [9] validated a force tracking test 309 and a joint-movement tracking test for the hand and rec-310 ommended to extend similar procedures to other joints. We 311 were able to find only few studies on elbow flexors [3,14,15], 312 and one on plantar flexors tracking ability [6], but none on 313 multi-joint closed-kinetic chain functional movement such 314 as simulated half squat. As a speculation, since lower limb 315 muscles would behave very similarly during the eccentric-316 concentric actions considered here and during descending-317 ascending stairs, these findings would prove useful for inves-318 tigating motor control and for identifying possible risk fac-319 tors for falls in particular populations (e.g., elderly, obese). 320 In turn, it should also be interesting to examine the effect of 321 322 trajectory-tracking training as a means of preventing falls in these individuals. 323

A new tracking-trajectory test for the assessment of mo-324 tor coordination has been proposed in the present study. The 325 main outcome (S.D. error) has been shown to be reliable and 326 sensitive to detect enhancement of tracking performance with 327 repeated trials in healthy female individuals. Since the sam-328 329 ple size used in this study is small, the generalizability of the results – for example to male subjects – is limited. It is 330 nevertheless interesting to conjecture that, if gender differ-331 ences in a lower limb task are similar to those reported for 332 finger movements [7], i.e., men tracked significantly more ac-333 curately than women, test-retest reliability would be greater 334 in male individuals. Potential applications of this test should 335 be in the area of exercise physiology (e.g., to study the ef-336 fect of fatigue, training or gender, see [7]), motor control 337 (e.g., to investigate brain plasticity after tracking practice or 338 training in both able-bodied and unhealthy individuals, see 339 [12,16]) and sports medicine (e.g., in rehabilitation settings, 340

where the horizontal leg press machine considered here is 341 commonly used). The present test should be improved by 342 concomitant quantification of the electromyographic activ-343 ity of the muscles involved in the tracking task (see [5]) and 344 by increasing the resistance on the leg press machine, in or-345 der to evaluate force control in addition to movement control 346 [9]. 347

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